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INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification 5 : G01R 33/38		A1	(11) International Publication Number: WO 92/07279 (43) International Publication Date: 30 April 1992 (30.04.92)
<p>(21) International Application Number: PCT/GB91/01758</p> <p>(22) International Filing Date: 10 October 1991 (10.10.91)</p> <p>(30) Priority data: 9022145.8 11 October 1990 (11.10.90) GB</p> <p>(71) Applicant (<i>for all designated States except US</i>): OXFORD INSTRUMENTS LIMITED [GB/GB]; Old Station Way, Eynsham, Oxford OX8 1TL (GB).</p> <p>(72) Inventor; and</p> <p>(75) Inventor/Applicant (<i>for US only</i>) : HANLEY, Peter [GB/GB]; Western Lodge, Parkend, Forest Of Dean, Gloucestershire GL15 4J0 (GB).</p> <p>(74) Agent: GILL JENNINGS & EVERY; 53/64 Chancery Lane, London WC2A 1HN (GB).</p>		<p>(81) Designated States: AT (European patent), BE (European patent), CH (European patent), DE (European patent), DK (European patent), ES (European patent), FR (European patent), GB (European patent), GR (European patent), IT (European patent), JP, LU (European patent), NL (European patent), SE (European patent), US.</p> <p>Published <i>With international search report.</i></p>	
<p>(54) Title: MAGNETIC FIELD GENERATING ASSEMBLY</p>			
<p>(57) Abstract</p> <p>A magnetic field generating assembly for use in NMR apparatus comprises a pair of first magnets (1, 2) with lines joining north-south poles of the magnets positioned along an axis with like poles facing one another. A pair of second magnets (3, 4) are positioned with lines joining their north-south poles substantially parallel with the axis. The positions and field strengths of the magnets (1, 2, 3, 4) are chosen so that a resultant field of controlled characteristics suitable for an NMR experiment is generated. The field (9) is generated in a working volume (8) spaced from the assembly. The magnets (1, 2, 3, 4) of the assembly are relatively adjustable along the axis.</p>			

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MAGNETIC FIELD GENERATING ASSEMBLY

The invention relates to a magnetic field generating assembly for use in nuclear magnetic resonance (NMR) apparatus and in particular to such apparatus for use in 5 well-logging applications.

It is well known that NMR can be used to inspect the geology around a bore hole. This is achieved by projecting a substantially uniform magnetic field into the rock surrounding the bore hole using a suitable field generator 10 and then performing an NMR experiment within the projected region. Commercial well-logging tools make use of the Earth's magnetic field but this is not a satisfactory technique and is particularly unsuitable for inspecting the so-called "uninvaded zone" surrounding the bore hole. The 15 uninvaded zone is that zone where there is no drilling fluid.

EP-A-0295134 describes apparatus and methods which seek to improve upon the earlier methods using the Earth's magnetic field. In this apparatus, four magnets are 20 provided positioned with their north-south directions lying on a common axis and with the north-south directions of the outer magnets and inner magnets respectively being opposed. The magnets are fixed to one another for ease of movement along a bore hole. The electrical coil required to 25 generate an rf magnetic field so as to perform the NMR experiment is mounted around the magnets.

This known arrangement suffers from a number of problems. Since there is magnetic material in the centre of the apparatus, this reduces the field strength in the 30 working volume projected outside the apparatus. Furthermore, positioning the rf coil around the magnets forces the designer to choose a non-conducting magnet material to avoid effects due to eddy-currents and noise coupling. This limits the magnet materials in practice to 35 permanent magnet materials such as ferrites and so prevents the use of materials now available with up to three times the strength which would enable measurements to be made at

greater distances into the rock. In addition, it is not feasible for producing large sensitive volumes because no provision is made for adjusting errors due to non-uniformities in the materials used and other differences 5 between the as manufactured and designed arrangement.

An earlier approach is described in US-A-4350955. In this case, just two magnets are provided spaced apart with their north-south axes aligned and with like poles facing one another. This arrangement has the advantage that the 10 rf coil can be positioned in the space between the magnets with the consequence that the magnets themselves can be made of non-permanent materials. However, the placement of the magnets is intrinsically less efficient than in EP-A-0295134. Although the arrangement of US-A-4350955 15 offers good vertical resolution (typically a few centimetres) it is not possible to change the radius of the working region in any convenient way. The ability to make measurements at several different distances into the rock is generally a requirement. Further, it has been reported 20 that the apparatus of US-A-4350955 can take 18 hours to measure one point. This is completely unacceptable in a practical well-logging situation.

In accordance with one aspect of the present invention, a magnetic field generating assembly for use in 25 NMR apparatus comprises a pair of first magnets, lines joining the north-south poles of the magnets being positioned along an axis with like poles facing one another; and at least one pair of second magnets positioned with lines joining their north-south poles substantially 30 parallel with the axis, wherein the positions and field strengths of the magnets are chosen so that a resultant field of controlled characteristics suitable for an NMR experiment is generated in a working volume spaced from the assembly and is characterised in that the magnets are 35 relatively adjustable in the axial direction.

We have devised a very significant improvement on the apparatus shown in EP-A-0295134. One major limitation of

that earlier approach is that the relative positions of the magnets are fixed. By permitting the magnets to be adjustable it is possible to achieve a significant increase in field strength in the working volume and to increase the 5 size of the volume which is subjected to a particular field strength. The method of the present invention results in improved homogeneity of the toroidal zone with greater flexibility. In a further refinement, it is also possible to obtain several different working volumes simultaneously.

10 This is achieved by using the second magnets to balance all or some of the non-zero order components of the fields generated by the first magnets in the working volume(s). The radial field uniform zone around the circumference of the toroidal zone of interest can be 15 controlled by the addition of a single pair of magnets. To control a series of increasing orders of derivatives of field with radial distance further pairs of magnets can be added. The contiguous pole faces of the prior art have a strong demagnetising effect on each other making control of 20 a long series of orders difficult. In one application, substantially all of the non-zero order components are balanced so that the field in the working volume(s) is substantially uniform. However, in one important application, it is possible to design the assembly so that 25 at least the first order and possibly other orders are not cancelled or significantly reduced so that a gradient field of known characteristics is generated in the working volume. It is well known that a gradient magnetic field enables spatial resolution to be achieved within the 30 working volume when performing NMR experiments.

A further advantage of the assembly is that the magnets can be arranged such that there is a space at the centre of the assembly into which an rf coil can be positioned. This enables at least the axially outer 35 magnets to be constructed from non-insulating material. RF transmit/receive coils can be air cored and therefore made of a wider choice of materials without coupling to the

receiver coil and inducing noise into the receiver system or damping the transmitter circuit.

Typically, the second magnets will be positioned axially inwardly with respect to the first magnets.

5 Further, there may be more than two first or second magnets.

In general, the inner magnets, usually the second magnets, will be permanent magnets, usually made of ferrite material, while the axially outer magnets, usually the 10 first magnets, can be permanent magnets, resistive electromagnets or superconducting magnets.

Typically, the assembly will be symmetrical about a mid-plane orthogonal to the axis although this may not always be the case.

15 Typically, the assembly further comprises a support to which the magnets are adjustably mounted. For example, each magnet could be connected to the support by a bracket which can be bolted to the support in a variety of positions. In another example, the magnets could be 20 mounted to a common lead screw via suitable connectors, rotation of those connectors causing the magnets to move longitudinally parallel with the lead screw.

As has already been mentioned, the invention is 25 particularly applicable to NMR apparatus which comprises a magnetic field generating assembly according to the first aspect of the invention, and an electrical coil for generating an rf magnetic field positioned at the centre of the assembly.

The invention also provides well-logging apparatus 30 comprising a magnetic field generating assembly according to the first aspect of the invention, the assembly being shaped so as to be movable along a bore hole, and an electrical coil for generating an rf magnetic field positioned at the centre of the assembly.

35 In accordance with a second aspect of the present invention, a method of constructing a magnetic field generating assembly for use in NMR apparatus comprises

positioning a pair of first magnets with the lines joining their north-south poles lying along an axis with like poles facing one another; positioning at least one pair of second magnets with lines joining their north-south poles substantially parallel with the axis; determining the field profile in a working volume spaced from the assembly due to the first magnets; and selecting the field strengths and positions of the second magnets so that a resultant field of controlled characteristics suitable for an NMR experiment is generated in the working volume.

An example of well-logging apparatus according to the invention will now be described with reference to the accompanying drawings, in which:-

Figure 1 is a schematic view of the apparatus;

Figures 2a-2c illustrate graphically the variation of magnetic field strength with radius for separate magnets and the combined magnet system in Figure 1, respectively; and,

Figure 3 illustrates graphically the variation in magnetic field strength for generating two working volumes of substantially uniform field, and the generation of a gradient magnetic field within a working volume.

The apparatus shown in Figure 1 comprises a pair of main, first magnets 1,2 positioned coaxially with their north poles facing one another. The magnets 1,2 are mounted by means not shown to a support 6. Axially inwardly of the magnets 1,2 are mounted a pair of second, auxiliary magnets 3,4 with their north-south axes coaxial with the axis defined by the magnets 1,2. The direction and magnetization strength of the magnets 3,4 is selected from a knowledge of how the different gradients vary. The magnets 1-4 are generally symmetrically positioned about a mid-plane orthogonal to the axis and an rf coil 5 is positioned between the magnets 3,4 at the mid-plane. The coil 5 is used during an NMR experiment in a conventional manner firstly to generate an rf magnetic field and then to act as a receiver to monitor rf signals generated by the

precessing nuclei as they relax back to their original state. The coil 5 is connected to conventional NMR processing electronics (not shown) while the support 6 is connected to a mechanism (not shown) which drops the 5 assembly down through a bore hole 7. As will be explained in more detail below, the magnets 1-4 are positioned and have field strengths such that a toroidal working volume 8 is generated within the rock strata surrounding the bore hole 7, the magnetic field within the working volume 8 being sufficiently uniform to perform an NMR experiment. 10 In some examples, additional working volumes could be generated radially spaced apart.

The radial field profile generated by the magnet 1 is shown schematically in Figure 2a and that produced by the 15 magnet 3 is shown in Figure 2b. Figure 2a shows that the main, powerful magnet 1 produces a peak field at a relatively large radius r_2 and Figure 2b shows the weaker magnet 3 producing a peak at a smaller radius r_1 . Figure 2c shows the sum of these components where the relative strength and positions of the two pairs of magnets are such 20 that a uniform region of field 9 has been produced centered about a radius r_0 .

To design such a system, it is convenient to express the magnetic field B at r_0 as a Taylor expansion:

$$B(r-r_0) = B(r_0) + \frac{dB}{dr} \Big|_{r_0} (r-r_0) +$$

25

$$\frac{d^2B}{dr^2} \Big|_{r_0} \frac{(r-r_0)^2}{2!} + \text{etc}$$

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To achieve the region of uniformity, we choose the magnets such that the individual gradients, $\frac{d^2B}{dr^2}$ sum to zero for the assembly of magnets. It should be 5 noted that the technique is not restricted to two pairs of magnets: for more complex systems we have sufficient degrees of freedom to cancel higher order gradients thereby resulting in a greater volume of uniformity. It should 10 also be noted that if required, we could leave a residual first order gradient, to provide spatial information in the NMR signal, so that in the received signal, the location of the source of signal would be such that $(f - f_0) = g.G.(r - r_0)$ where G is the strength of the first order gradient and g is the gyro magnetic ratio for the nuclei being 15 detected. This technique is familiar to those skilled in magnetic resonance imaging or zeugmatography. Such a first order gradient could also be used to measure diffusion effects by techniques that are well known in NMR spectroscopy.

20 In the description that follows, the discussion is appropriate to uniformly magnetised permanent magnets. Similar descriptions can be obtained for air-cored coils etc., and non-uniform magnetisation can be modelled using a superposition of several magnets of differing 25 magnetisation.

We begin by calculating the field due to a thin magnetised bar. This simplifies the mathematical discussion but it can be readily extended to a general form.

$$\phi = \frac{1}{4\pi\mu} \int M \cdot \nabla \left(\frac{1}{s} \right) dV$$

volume of magnetised material

5 We define a field point $\bar{p} = (x, y, z)$ and a source point $\bar{q} = (u, v, w)$. Then $\bar{s} = \bar{p} - \bar{q} = (x-u, y-v, z-w)$.

Let the magnetization be in the z-direction so $M = (0, 0, M)$.

$$\phi = \frac{-M}{4\pi\mu} \int \frac{\partial}{\partial w} \left(\frac{1}{s} \right) dV$$

$$\phi = \frac{-AM}{4\pi\mu} \int \frac{(z-w) dw}{s^3}$$

10 Let the magnetic material be confined to a thin bar of cross-sectional area A, lying along the z-direction so $\bar{q} = (0, 0, w)$.

The field is then given by

$$\bar{H} = -\nabla_{\bar{p}} \phi$$

15 $\bar{B} = \mu \bar{H}$

$$\bar{B} = \frac{AM}{4\pi} \nabla \left| \frac{1}{(x^2+y^2+(z-w)^2)^{1/2}} \right|_{w_1}^{w_2}$$

In cylindrical polar coordinates:

$$\bar{B} = \frac{AM}{4\pi} \nabla \left| \frac{1}{(r^2+(z-w)^2)^{1/2}} \right|_{w_1}^{w_2}$$

from which

$$B_z = \frac{AM}{4\pi} \left| \frac{z-w}{(r^2+(z-w)^2)^{3/2}} \right|_{w_1}^{w_2}$$

$$B_x = \frac{AM}{4\pi} \left| \frac{x}{(x^2 + (z-w)^2)^{3/2}} \right| \frac{w_2}{w_1}$$

In our system of opposed magnets, symmetric about the $z = 0$ plane, the H_z 's cancel and the H_r 's reinforce, hence

$$B = B_x = \frac{AM}{2\pi} \left| \frac{x}{(x^2 + w^2)^{3/2}} \right| \frac{w_2}{w_1}$$

$$\frac{dB_x}{dx} = \frac{AM}{2\pi} \left| \frac{w^2 - 2x^2}{(x^2 + w^2)^{5/2}} \right| \frac{w_2}{w_1}$$

$$\frac{d^2B_x}{dx^2} = \frac{AM}{2\pi} \left| \frac{x(6x^2 - 9w^2)}{(x^2 + w^2)^7/2} \right| \frac{w_2}{w_1}$$

etc.

The above description is only accurate for thin magnets, whose radii are much less than the radial position of the field point at which the magnetic field is measured. An exact representation which however requires rather more 5 computational effort is provided by the current sheet model.

Text books on electromagnetism show that a uniformly magnetised solid can be replaced by a closed sheet over its surface carrying a current density whose direction is perpendicular to that of the magnetisation. This 10 representation is exact (so long as the magnetisation is uniform and unidirectional) and straightforward to deal with in the case of axially magnetised cylindrical objects. In this case, the external field is that of a solenoid of zero thickness. Expressions (and computer code) for this exist 15 and generally require integrating the field due to an elementary hoop with respect to length, polar angle and radial thickness. In the case of a current sheet we may omit integration with respect to radius so that:

$$B_z = \frac{M}{4\pi} \left| \int_0^{2\pi} \frac{a \cos(\phi) d\phi}{((z-b)^2 + r^2 + a^2 - 2a \cos(\phi))^{1/2}} \right|_{w_1}^{w_2}$$

20 $B_z =$

$$\frac{M}{4\pi} \left| \int_0^{2\pi} \frac{a(z-w) (a - r \cos(\phi)) d\phi}{(r^2 + a^2 - 2a \cos(\phi)) ((z-w)^2 + r^2 + a^2 - 2a \cos(\phi))^{1/2}} \right|_{w_1}^{w_2}$$

Where we have also replaced the solenoidal current density, $j/10$ (j in Amperes/cm²) with the magnetisation $M/4\pi$ (M in gauss per cm³), the dimensions becoming correct from 25 the absence of the integration over "a".

The ϕ integral is done by substituting $\theta = \phi/2$ and using the numerical evaluation of the elliptic integral

$$CEL(K_c, p, a, b) = \int_0^{\pi/2} \frac{(\cos(\theta) + b \sin(\theta)) d\theta}{(\cos^2(\theta) + p \sin^2(\theta)) (\cos^2(\theta) + k_c^2 \sin^2(\theta))^{1/2}}$$

10a

(Bulirsch, Numerical Math, vol 9, 305 (1969) Using
this method, the radial field derivatives may be obtained
by numerical differentiation.

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Example

A magnet system to produce a field peak of 50 gauss at a radial distance of 40cm has $w_1 = 56\text{cm}$, $w_2 = 206\text{cm}$ and $MA = 2.5 \cdot 10^6 \text{ gauss-cm}^2$. This could be made from Nd-
 5 Fe-B alloy, 16cm in diameter and with a magnetisation of 12500 gauss. This produces a sensitive region whose radial extent (uniform to 1 in 10^3) is about 2cm.

Below are tabulated the gradient functions for unit value of AM at 30cm radius. In the same table are included
 10 the gradient functions for a magnet with $w_1 = 10.3\text{cm}$ and $w_2 = 11.3\text{cm}$. It should be noted that the ratio of dB/dr to d^2B/dr^2 are the same for the two systems, but the signs of the individual gradients are different.

$w_1=56$	$w_2=206$	$\frac{dB}{dr}$	$\frac{d^2B}{dr^2}$	$\frac{dB}{dr} / \frac{d^2B}{dr^2}$
$+3.000E+01$	$+1.137E-04$	$+1.187E-06$	$-1.633E-07$	$-7.270E+00$

$w_1=10.3$	$w_2=11.3$	$\frac{dB}{dr}$	$\frac{d^2B}{dr^2}$	$\frac{dB}{dr} / \frac{d^2B}{dr^2}$
$+3.000E+01$	$+2.948E-05$	$-3.367E-06$	$+4.634E-07$	$-7.265E+00$

15

By choosing the strength of the smaller magnet to be 0.3525 that of the larger we get cancellation of the first and second order gradients.

Element # or 0	1.000E+000
20 M.A. gauss	2.500E+006
w1 cm	5.600E+001
w2	2.060E+002
Element # or 0	2.000E+000
M.A. gauss	8.813E+005
25 Z1 cm	1.030E+001
Z2	1.130E+001

11a

<i>R</i>	Br	dBr/dr	d^2Br/dr^2	d^3Br/dr^3
3.000E+001				
4.523E+001	4.723E-001	-6.496E-002	2.256E-003	
4.135E000	-4.722E-001	6.500E-002	-1.030E-002	
total	4.937E+001	1.265E-004	3.199E-005	-8.039E-003

$$\frac{d^4Br}{dr^4}$$

1.166E-004
2.497E-003
2.614E-003

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Figure 3 shows at 10 the magnetic field plotted against radial distance for the combination with two pairs of magnets.

5 By including more magnets in the system, higher order gradients could be cancelled thereby increasing the volume of uniformity still further. Graph 11 shows the results for three pairs of magnets and graph 12 is that for three pairs with a first order gradient.

10 Because the smaller magnet is weaker, it can be made of ferrite so that its proximity to the RF coil does not cause any problems with coupling. For example, a 16cm diameter disc of ferrite with magnetisation 4380 gauss will achieve the desired effect.

15 To compensate for manufacturing errors, additional discs of ferrite can be added to (or removed from) the small magnet to get the correct ratio of strengths, and axial movements can be made to achieve the correct ratio of gradients.

20 The magnets 3,4 will typically be made of a permanent magnet material such as ferrite but the magnets 1,2 could be permanent magnets, resistive magnets or superconductive magnets.

When more than two pairs of magnets are included in the system, in order to cancel higher order gradients, it becomes more difficult to balance the ratios of the gradients in the way described above. An alternative method is to seek a 5 minimum in a function such as

$$|k_1 [H_1 - \sum_j h_1(w_{1j}, w_{2j}, M_j)]^2 + k_2 [H_2 - \sum_j h_2(w_{1j}, w_{2j}, M_j)]^2 +$$

$$k_3 [H_3 - \sum_j h_3(w_{1j}, w_{2j}, M_j)]^2 + \text{etc}|^4$$

Where the H_k are the gradients of the main magnet to be cancelled and the $h_k(w_{1j}, w_{2j}, M_j)$ are the gradients of the 10 correcting magnets whose ends are at $z = w_1$ and $z = w_2$ and whose strength is M . The constants K_k are weighting factors for each order of gradient. The minimum or minima can be found using computer programs which rely on well-known methods such as "simulated annealing" or "steepest slope".

15 The gradients due to a system comprising three pairs of magnets found in this way are tabulated below. It should be noted that this has allowed substantial reduction in the 3rd and 4th order gradients compared with the system of two pairs described above. It should also be noted that one pair of 20 magnets is magnetised in opposition to the other two pairs.

Element # or 0 1.000E+000

M.A. gauss 2.413E+006

W1 cm 5.600E+001

W2 2.060E+002

25 Element # or 0 2.000E+000

M.A. gauss 4.172E+005

W1 cm 1.950E+001

W2 2.463E+001

Element # or 0 3.000E+000

30 M.A. gauss -6.722E+005

W1 cm 3.653E+001

W2 4.435E+001

13a

<i>R</i>	3.000E+001	<i>HO</i>	<i>dBr/dr</i>	<i>d²Br/dr²</i>	<i>d³Br/dr³</i>
4.366E+001	4.366E+001	4.559E-001	-6.270E-002	2.177E-003	
9.423E+000	9.423E+000	-7.081E-001	5.337E-002	-2.804E-003	
-9.479E+000	-9.479E+000	2.516E-001	8.935E-003	-2.466E-003	
total	4.360E+001	-6.310E-004	-4.003E-004	-3.093E-003	

d⁴Br/dr⁴
1.125E-004
2.172E-004
1.981E-004
5.278E-004

Figure 3 shows at 11 a uniform field generated from three pairs of magnets.

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The same procedure can be used to design magnet systems where a gradient is deliberately introduced. This may be done so as to

5 a) provide spatial information from the sensitive region using the well-known techniques of magnetic resonance imaging.

10 b) optimise the radio-frequency pulse over the complete sensitive region (which now has a large radial extent in these compensated systems) to compensate for the non-uniformity of the field produced by the transmitter coil by providing a pulse or series of pulses whose intensity varies with frequency in such a way as to provide this compensation via the gradient's imposing a relationship between resonant frequency and radius.

15 For example, a first order gradient can be introduced by subtracting the required gradient from the value of H_1 used in the function to be minimised.

20 A typical result where a first-order gradient of 0.1 gauss per cm. has been deliberately introduced is shown below:

Element # or 0 1.000E+000
M.A. gauss 2.413E+006
W1 cm 5.600E+001
W2 2.060E+002
25 Element # or 0 2.000E+000
M.A. gauss 3.200E+005
W1 cm 2.050E+001
W2 2.889E+001
Element # or 0 3.000E+000
30 M.A. gauss -6.803E+005
W1 cm 3.601E+001
W2 5.109E+001

14a

<i>R</i>	3.000E+001	<i>HO</i>	<i>dBr/dr</i>	<i>d²Br/dr²</i>	<i>d³Br/dr³</i>
		4.366E+001	4.559E-001	-6.270E-002	2.177E-003
		1.070E+001	-7.172E-001	4.440E-002	-9.708E-004
		-1.593E+001	3.611E-001	1.806E-002	-3.842E-003
total	3.843E+001		9.980E-002	-2.394E-004	-2.636E-003

<i>d⁴Br/dr⁴</i>
1.125E-004
-8.788E-005
2.663E-004
2.909E-004

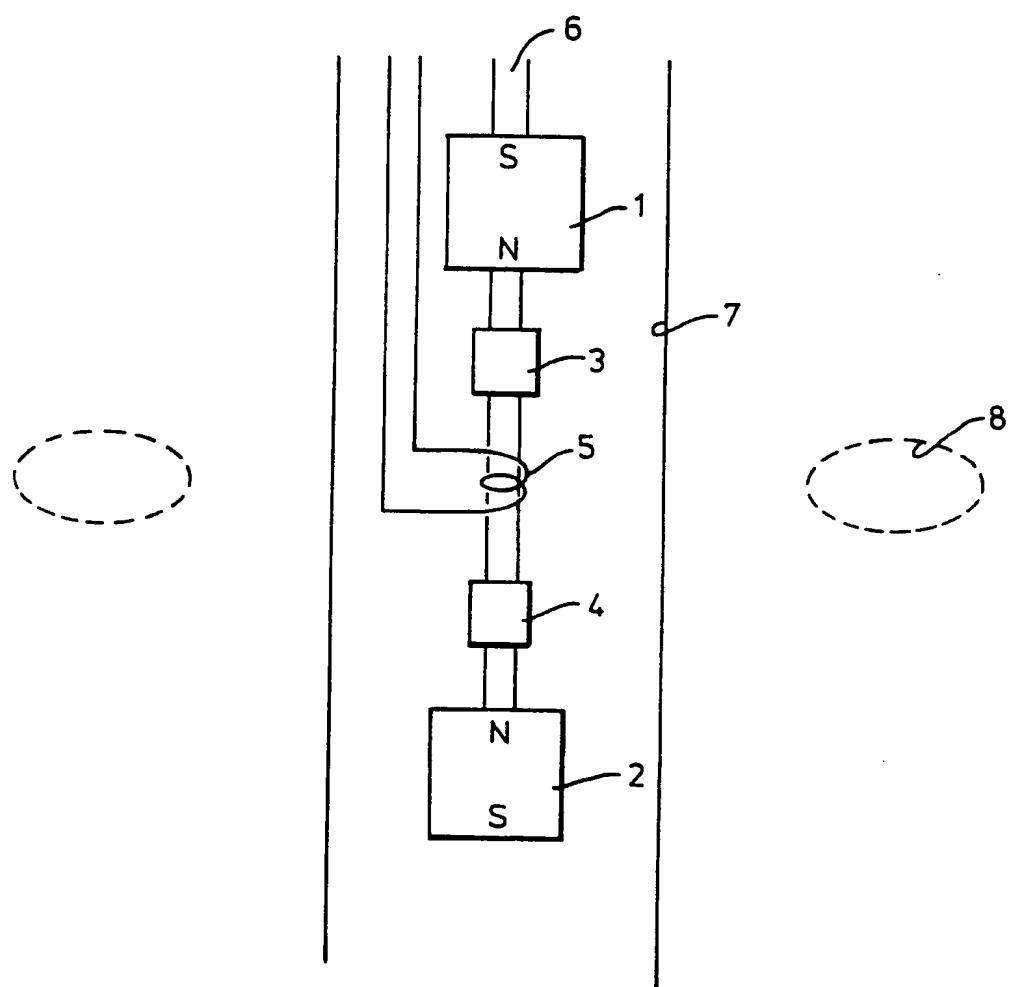
Figure 3 shows the profiles of field versus radius for the three magnet systems described above. Note that the
5 remanent third order gradient produces a subsidiary maximum at a smaller radius. The relatively uniform field at this maximum can be used as a second sensitive region, and because it is closer to the RF coil than the main region it does not need to be so big to provide adequate signal
10 strength. Because resonance occurs at a different frequency, this can be excited independently and so information can be obtained from two regions simultaneously.

CLAIMS

1. A magnetic field generating assembly for use in NMR apparatus, the assembly comprising a pair of first magnets (1,2), lines joining the north-south poles of the magnets (1,2) being positioned along an axis with like poles facing one another; and at least one pair of second magnets (3,4) positioned with lines joining their north-south poles substantially parallel with the axis, wherein the positions and field strengths of the magnets are chosen so that a resultant field of controlled characteristics suitable for an NMR experiment is generated in a working volume spaced from the assembly characterised in that the magnets are relatively adjustable in the axial direction.
2. An assembly according to claim 1, wherein the resultant field in the working volume (8) has a first order gradient in the radial direction.
3. An assembly according to claim 1 or claim 2, wherein the second magnets (3,4) are provided axially inwardly of the first magnets (1,2).
4. An assembly according to any of the preceding claims, wherein the second magnets (3,4) are permanent magnets.
5. An assembly according to any of the preceding claims, wherein the first magnets (1,2) are permanent magnets, resistive electromagnets, or superconducting magnets.
6. An assembly according to any of the preceding claims, wherein the positions and field strengths of the second magnets (3,4) are chosen so as to reduce or cancel non-zero order components of the magnetic fields generated by the first magnets (1,2).
7. An assembly according to any of the preceding claims, further comprising a support to which the magnets (1,2,3,4) are adjustably mounted.
8. NMR apparatus comprising a magnetic field generating assembly according to any of the preceding claims; and at least one electrical coil (5) for generating and detecting an rf magnetic field, the coil being positioned at the centre of the assembly.

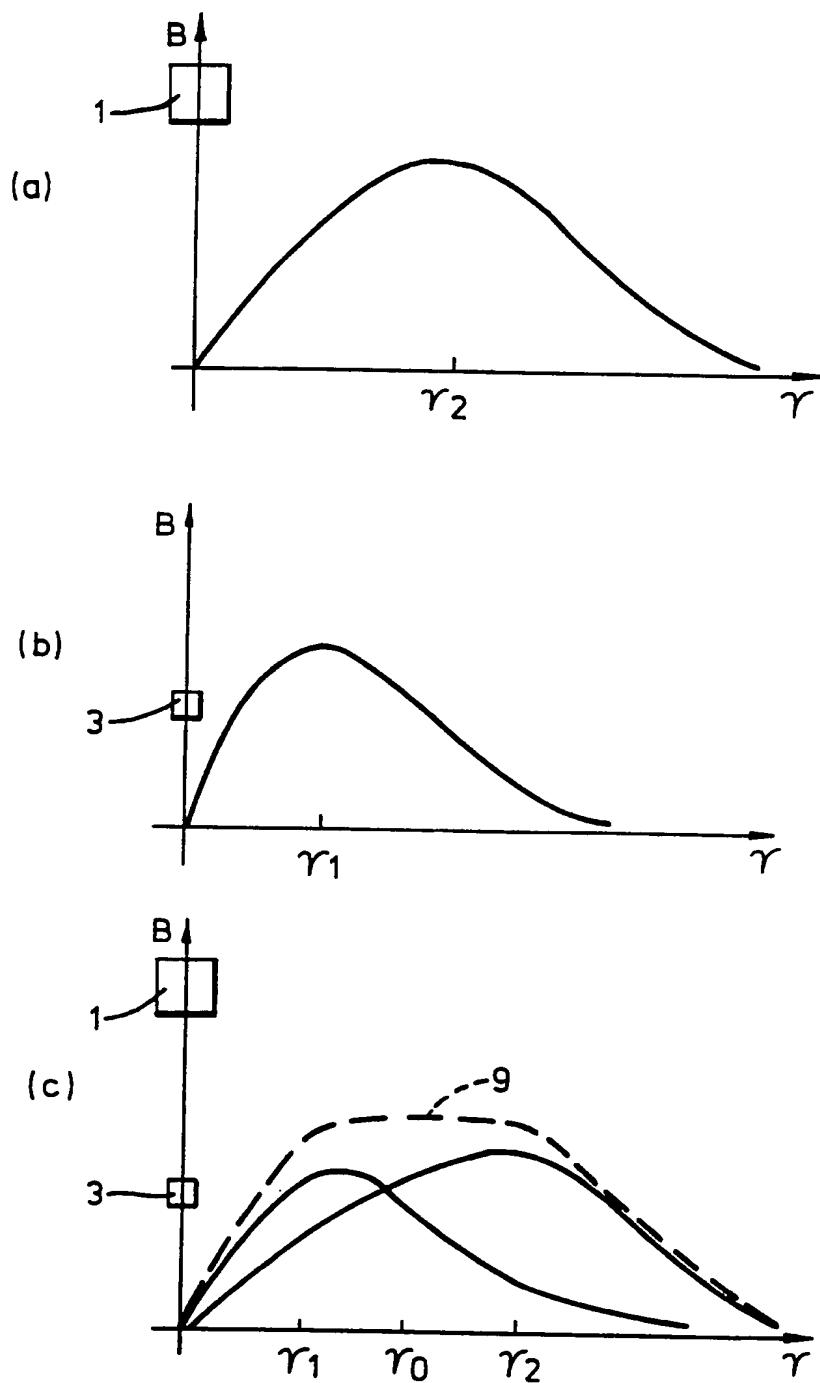
9. Apparatus according to claim 8, wherein the magnets are axially spaced from a central region which is surrounded by the electrical coil.
10. Well-logging apparatus according to claim 8 or claim 5 9.
11. A method of constructing a magnetic field generating assembly for use in NMR apparatus, the method comprising positioning a pair of first magnets (1,2) with the lines joining their north-south poles lying along an axis with 10 like poles facing one another; positioning at least one pair of second magnets (3,4) with lines joining their north-south poles substantially parallel with the axis; determining the field profile in a working volume (8) spaced from the assembly due to the first magnets (1,2); 15 and selecting the field strengths and positions of the second magnets (3,4) so that a resultant field of controlled characteristics suitable for an NMR experiment is generated in the working volume.

Fig.1.



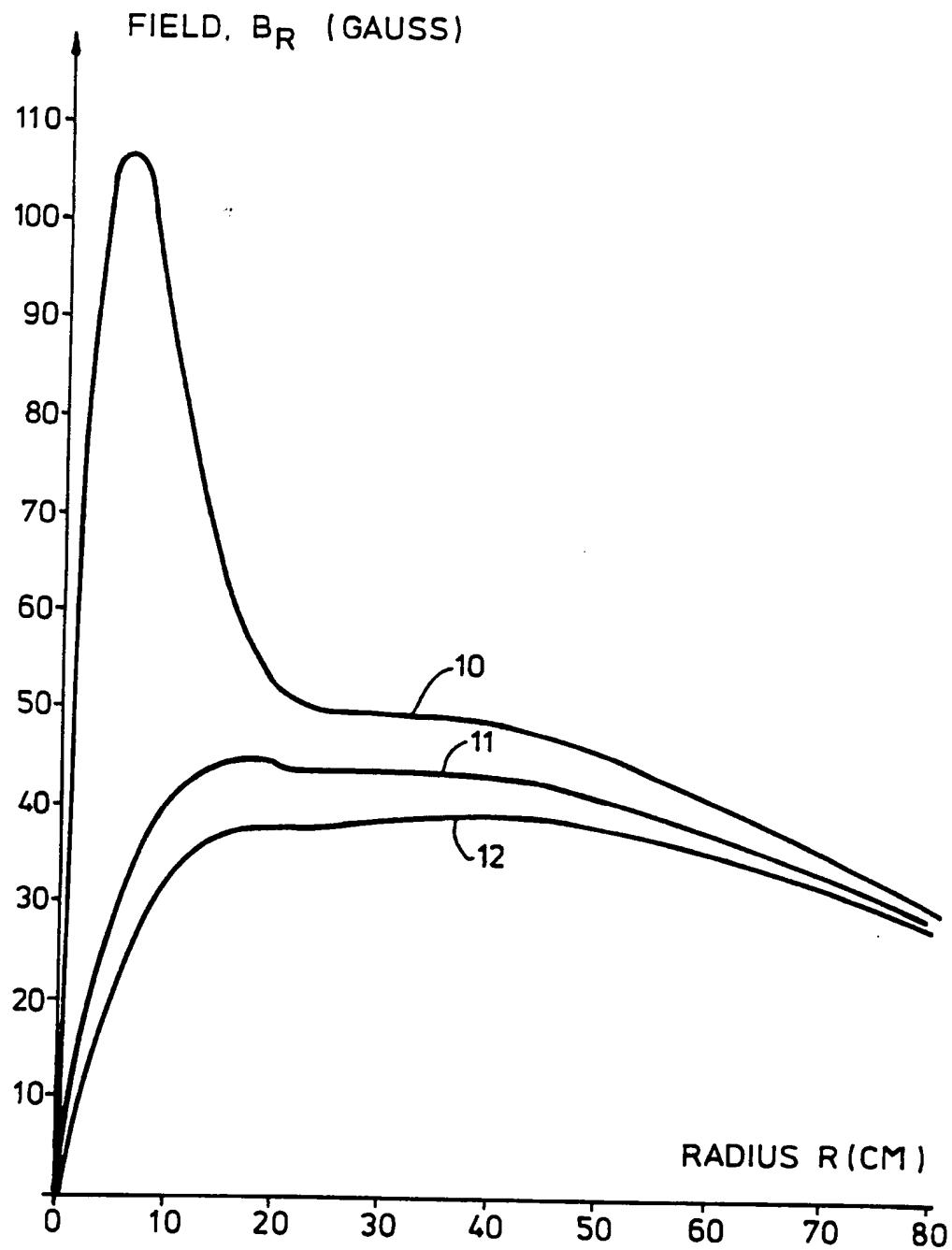
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Fig. 2.



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Fig. 3.



INTERNATIONAL SEARCH REPORT

International Application No

PCT/GB 91/01758

I. CLASSIFICATION OF SUBJECT MATTER (if several classification symbols apply, indicate all)⁶According to International Patent Classification (IPC) or to both National Classification and IPC
Int.Cl. 5 G01R33/38

II. FIELDS SEARCHED

Minimum Documentation Searched⁷

Classification System	Classification Symbols	
Int.Cl. 5	G01R ;	G01V ; H01F

Documentation Searched other than Minimum Documentation
to the Extent that such Documents are Included in the Fields Searched⁸III. DOCUMENTS CONSIDERED TO BE RELEVANT⁹

Category ¹⁰	Citation of Document, ¹¹ with indication, where appropriate, of the relevant passages ¹²	Relevant to Claim No. ¹³
A	EP,A,0 295 134 (NUMAR CORPORATION) 14 December 1988 cited in the application see column 4, line 17 - column 5, line 45 see column 6, line 23 - column 7, line 28 see figures 1,3 ---	1,3-5,8, 10,11
A	US,A,4 350 955 (J.A. JACKSON, R.K. COOPER) 21 September 1982 cited in the application see column 2, line 38 - line 68 see column 4, line 47 - line 59 see column 6, line 7 - line 32 see figures 1,2,6 ---	1,2,7-11
A	GB,A,2 141 236 (NATIONAL RESEARCH DEVELOPMENT CORPORATION) 12 December 1984 see the whole document ---	1,4,5, 7-11

¹⁰ Special categories of cited documents :

"A" document defining the general state of the art which is not considered to be of particular relevance
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 "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
 "O" document referring to an oral disclosure, use, exhibition or other means
 "P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
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 "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.
 "A" document member of the same patent family

IV. CERTIFICATION

Date of the Actual Completion of the International Search

03 JANUARY 1992

Date of Mailing of this International Search Report

24.01.92

International Searching Authority

EUROPEAN PATENT OFFICE

Signature of Authorized Officer

VOLMER W.

III. DOCUMENTS CONSIDERED TO BE RELEVANT (CONTINUED FROM THE SECOND SHEET)		
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A	WO,A,8 604 687 (FIELD EFFECTS, INC.) 14 August 1986 see page 4, line 30 - page 7, line 30 see page 14, line 32 - page 16, line 21 see figures 7,8 ---	1,2
A	EP,A,0 154 996 (KABUSHIKI KAISHA TOSHIBA) 18 September 1985 see page 7, line 9 - page 8, line 26 see page 10, line 33 - page 11, line 26 see page 13, line 24 - page 15, line 31 see figure 8 ---	1,2,6

ANNEX TO THE INTERNATIONAL SEARCH REPORT
ON INTERNATIONAL PATENT APPLICATION NO. GB 9101758
SA 51894

This annex lists the patent family members relating to the patent documents cited in the above-mentioned international search report. The members are as contained in the European Patent Office EDP file on The European Patent Office is in no way liable for these particulars which are merely given for the purpose of information. 03/01/92

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